

**MODELING OF FACI AND NaCl AEROSOL NEPHELIZATION AND RETENTION
IN RESPIRATORY SYSTEMS**

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ABSTRACT

The nebulization process is important to deposition and retention of soluble aerosols in the respiratory tract, in the very humid lung atmosphere. Soluble aerosols become droplets of solution and grow rapidly in dimension. The phase transition and nebulization rate of the coarse NaCl aerosols in transit through lung airways exhibit a completely different mode to that of practically the most environmentally hazardous acid aerosols. Previous animal retention studies had shown significant discrepancies in dose-response relationships among known subjects and aerosol species. Recent experimental measurements indicate that aerosol retention time in the lung plays the most important role for biological effect estimation. In the present work, a time-dependent retention model is used to present aerosol retention and to compare the effects due to inhaled soluble NaCl coarse MMD aerosols. Results show good agreement with most of published experimental data.

GENERAL MODELING METHOD

The effect of particle nebulization on the retention of inhaled soluble aerosols in the respiratory system has been studied in a broad manner. Several data indicate that only relative humidity (R.H.) plays an active role in nebulization and growth rate. Figure 1 shows that at any constant ambient temperature, behavior based on all NaCl aerosols exhibit the same trend for aerosol growth that is, for R.H. greater than 70%, the final diameter grows almost proportionally each other. Since R.H. in the respiratory tract is believed to be within the range of 90-95% [1], it is reasonable to expect the four aerosols to display similar nebulization patterns once the aerosol size has reached its terminal diameter prior to entering the trachea. Due to the Kelvin and hygroscopic effects, variation in NaCl aerosol size is different from that of MMD aerosols. In Figure 2, the solid curves show the effect of increasing R.H. on NaCl crystal, and the dashed curves represent the nebulization of NaCl. As R.H. is increased to above 70%, the NaCl crystal nebulization rate goes down whereas the droplets that continue to grow with increasing R.H. to R.H. decreases only 10%. The nebulization curves initially follow the nebulization curves, however, at R.H. of 75%, the NaCl droplets do not nebulize, but remain supersaturated until a much lower R.H. [2]. For simplicity, both NaCl and MMD aerosol final equilibrium sizes are determined by the median MMD-100 group's equation [3]:

$$d/d_0 = [\frac{1}{1 + (d/d_0)^3}]^{1/3} \frac{R/H - 70}{100} \quad (1)$$

where d and d_0 are, respectively, final and initial droplet size of the aerosol; μ and μ_0 are, respectively, final and initial retention; μ and μ_0 are, respectively, retention velocity of aerosol and that of the dry aerosol; μ is the R.H.; μ_0 is the effective number of ions produced by dissociation of a water molecule; and k is the Kelvin factor. Equation (1) shows that the effect of hygroscopicity on retention will be more significant for aerosols of compounds having high molecular weight and large diameter. For dry MMD, the density is 1.8 and the water content is about 60, both values being higher than those of NaCl which has a molecular

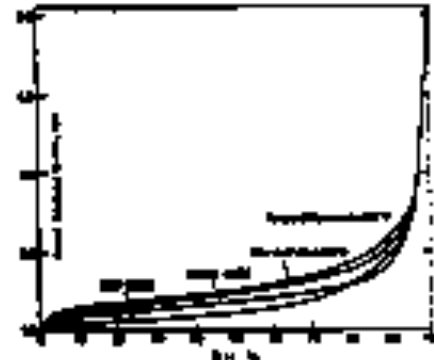


Fig 1. R.H. nebulization vs R.H.

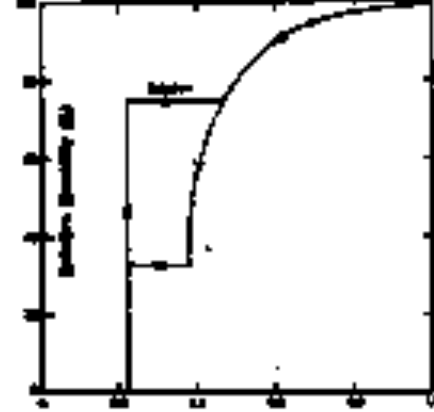


Figure 2. NaCl size vs R.H.

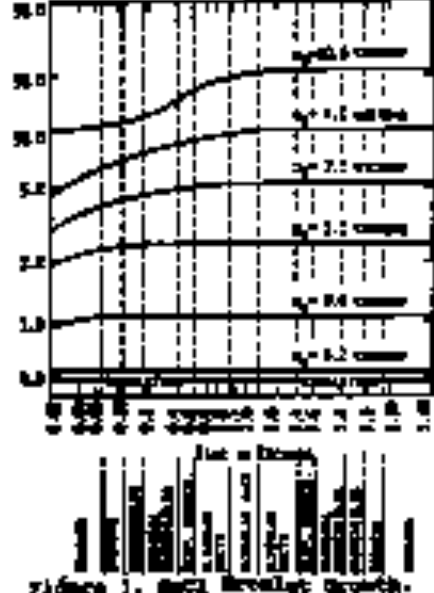


Figure 3. NaCl droplet growth.

weight of 50.5 and particle density of 1.2 at 25°C. Thus, calculations are more rapid for H₂O than in the case of NaCl. Shown in Figure 3 is the growth history of a NaCl aerosol in the human respiratory tract at various initial particle sizes calculated from equation (1). It is seen that aerosols of smaller initial sizes reach their equilibrium sizes quicker than do larger aerosols. Ultrafine aerosols with initial diameters smaller than 0.2 micron become wet soon when they enter the trachea, while coarse aerosols do not reach their final sizes at all during the breathing period. This suggests that the retention behavior of ultrafine hygroscopic aerosols in the human respiratory system may be different in the same way as non-hygroscopic aerosols, provided that the appropriate terminal diameters of the hygroscopic aerosols are used as simulated non-hygroscopic aerosols [4].

RETENTION CALCULATION & RESULTS

According to our previously detailed time-dependent retention model [5], aerosol deposition in each alveolar generation and bronchopneumonic aerosols from all succeeding generations can be described by Figure 4 and calculated as follows:

$$\text{Inflow: } -\left[\frac{t_{i+1} + t_i}{2} + t_i - t_{i+1}\right] \left[\frac{q_{i+1}}{t_{i+1}}\right] \quad (2)$$

$$\text{Outflow: } -\left[\frac{t_{i+1} + t_i}{2} + t_i - t_{i+1}\right] \left[\frac{q_{i+1}}{t_{i+1}}\right] \quad (3)$$

$$\text{at } t_i + t_{i+1} < t_{\text{exp}} \text{ for } i^{\text{th}} \text{ generation.}$$

where q and t are, respectively, aerosol deposition fraction and clearance time in each generation. i is the generation number, and t is total aerosol exposure time. Assuming a P.M. value of 0.9 throughout the entire respiratory tract, the distribution of NaCl aerosols of both 0.1 and 1.0 microns is shown in Figure 5, since the primary mechanism of 0.1-micron aerosol deposition is diffusion, retention for NaCl and non-hygroscopic aerosols exhibit similar patterns. For large aerosols with sizes greater than 0.2 micron, deposition mechanism may change from sedimentation to impaction due to hygroscopicity, thereby altering the retention pattern. Under various respiratory conditions, calculated NaCl aerosol retention curves well with experimental data [6,7], as shown in Figure 6. Due to the large subject variability commonly observed in retention measurements, inter-subject variability of the aerosol sizes below 0.1 micron. For one-hour exposure to H₂O aerosols, the three different concentrations on three different days, human alveolar clearance values obtained can be described by Figure 7. It is observed that the higher the H₂O dose, the lower the response due to stimulating effect; and a correlation exists as given in Figure 8. In a comparable H₂O exposure experiment on rabbits [8], it was also observed that increasing exposure concentration fits intrathoracic and then extrathoracic the sum of recirculatory clearance.

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Figure 4. Retention Retention Model.

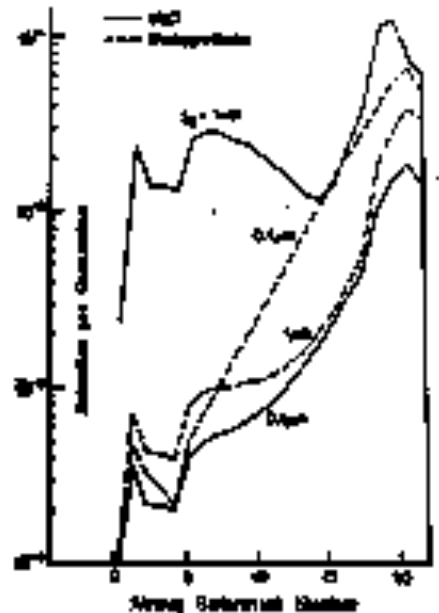


Figure 5. NaCl Retention in Highway.

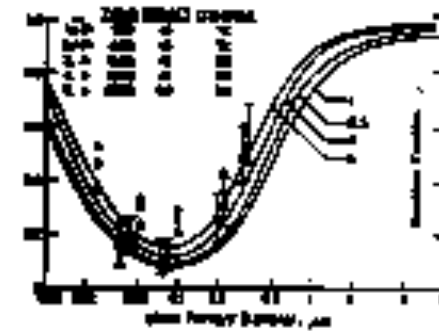


Figure 6. Clearance vs Dose.

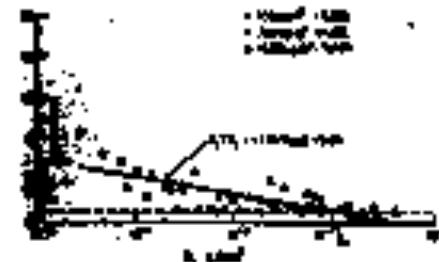


Figure 7. H₂O Dose-Response.